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Resonance Imaging (MRI) is a known technique for
producing images of the inside of the body of a
patient. MRI uses a strong magnetic field and radio
frequency (RF) pulses in order to excite the nuclei
of certain atoms, the atomic nuclei having been
placed in a static magnetic field by a sequence of
gradient magnetic fields. After the RF pulses, the
nuclei become excited and begin emitting signals,
which the MRI system detects and uses to construct
an image of the nuclei and thus the body parts in the
region of the nuclei. MRI systems typically include
a transmitter coil that is used to transmit RF
excitation pulses into a patient. A similar receiver

coil, which is commonly referred to as the “local coil,” is located in the vicinity of the patient to receive the emitted RF signals. When the patient is moved from one position to another, as when the patient is moved from one MRI system to another, the receiver coil has to be re-adjusted to correspond to the new position of the patient. The local coil receives both the RF signals emitted by the patient and the RF excitation pulses transmitted by the transmitter coil. The local coil also detects the emitted RF signals. This means that the local coil must be RF shielded to prevent the local coil from being exposed to electromagnetic interference (EMI) originating from the RF excitation pulses or from the transmitted RF signals. Unfortunately, the local coil cannot be RF shielded until the patient is placed in the MRI system. In the prior art, this can be accomplished by the technician manually

adjusting the local coil, for example, by raising or lowering the local coil into or out of the RF shield. Manual adjustment can take a relatively long time, for example, on the order of minutes or even hours. There is therefore a need for a method for more quickly and more reliably aligning an RF shielded local coil with a patient in an MRI system.

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